

IN THE SPECIFICATION

The paragraph beginning at page 2, line 8 has been amended as follows:

In a biplane x-ray arrangement with each employing an x-ray image intensified as the x-ray detector, it is comparatively simple to suppress the scattered radiation, because one x-ray system is always switched "blind", i.e. unreceptive to x-rays, while the other x-ray system is in operation. This has the disadvantage, however, that only temporally displaced x-ray exposures of a patient can be acquired with the two x-ray systems of the biplane x-ray device. A further disadvantage of this technique is that the possibility to switch blind is not present in x-ray detectors of the solid state type, ~~fore~~ for example aSi detectors. In this case, operation must be undertaken with a reduced image rate in both x-ray systems, which constrains the operator. The effective image rate that would otherwise be available thus is too high to select as the useable image rate, which means the systems must be operated below their technical capabilities.

The paragraph beginning at page 6, line 6, has been amended as follows:

The x-ray device schematically shown in Fig. 1 has two x-ray systems 1 and 2 that, in the exemplary embodiment, are adjustable around a patient P positioned on a schematically indicated patient positioning device 3. The x-ray system 1 has an x-ray source 4 as well as an x-ray detector 5, and the x-ray system 2 has an x-ray source 6 as well as an x-ray detector 7. The x-ray source 4 and the x-ray detector 5 as well as the x-ray source 6 and the x-ray detector 7 each are preferably arranged on a C-arm (not shown). The x-ray source 4 and the x-ray source 6 ~~each~~ respectively emit ~~[[a]] conical x-ray beam~~ beams 10 and 12. In the exemplary embodiment, the x-ray detectors 5 and 7 are solid-state detectors. The x-ray

systems 1 and 2 are connected to a calculating device 8. The calculating device 8, which controls the operation of the x-ray device, is additionally connected to memory 9 of the x-ray device.

The paragraph beginning at page 6, line 18, has been amended as follows:

In the operation of the x-ray device, x-ray exposures of a body region of the patient P can be acquired practically simultaneously from different angles with the two x-ray systems 1 and 2. As explained above, the scattered radiation which is emitted from the body of the patient P in all directions disadvantageously affects the quality of the x-ray recordings of the body region of the patient P acquired with the x-ray systems 1 and 2. The origin of the weaker energy x-ray radiation 11 scattered ~~[[n]]~~ in the body of the patient P is illustrated in Fig. 1 for the operation of the x-ray system 1, by an ~~an~~ the x-ray radiation beam 10 being emitted from the x-ray source 4 toward the direction of the patient P, as well as toward the x-ray detector 5. As can be seen in Fig. 1, although the scattered radiation 11 is not uniform, it nevertheless radiates in all directions as well as in the direction of the x-ray detector 7 of the x-ray system 2. The scattered radiation 11 contributes no useful information for the acquisition of x-ray images with the x-ray detector 7. Furthermore, the image quality ~~if~~ of the x-ray recordings acquired with the x-ray detector 7 is degraded by the scattered radiation 11. The same is true for scattered radiation which strikes upon the x-ray detector 5 of the x-ray system 1, when an x-ray beam is emitted from the x-ray source 6 of the x-ray system 2 in the direction of the patient P and the x-ray detector 7.

The paragraph beginning at page 8, line 5 has been amended as follows:

Preferably, a number of such x-ray scattered radiation images are acquired for the two x-ray detectors of the x-ray systems 1 and 2, and are averaged in an averaging unit 13, such that a resulting x-ray scattered radiation image is obtained which exhibits reduced statistical noise, for each x-ray system.

The paragraph beginning at page 8, line 21 has been amended as follows:

Normally, x-ray scattered radiation images for the two x-ray detectors 5 and 7 are determined and stored in the memory 9 for different positions of the x-ray systems 1 and 2 relative to one another in the previously described manner. The determination of the x-ray scattered radiation images thereby ensues according to defined acquisition conditions, such as x-ray spectra, x-ray dosages, and acquisition geometries. If, given the same position of the x-ray systems 1, 2 relative to one another and an unchanged position of the patient P on the patient positioning device 3, only the x-ray dosage changes, then no new x-ray scattered radiation image must be determined. ~~Since the~~ The x-ray scattered radiation images are proportional to the x-ray dosage[$[\cdot]$]. If the x-ray sources 4 and 6 emit x-rays at respectively different doses (as schematically indicated in Fig. 1 by the lower number of rays in the beam 12 compared to the beam 10), a scaling of the x-ray scattered radiation images corresponding to the change of the x-ray dosage can ensue in a scaling unit 14, and the respective x-ray scattered radiation images required for the subtraction can be determined in this manner.

The paragraph beginning at page 9, line 19 has been amended as follows:

As is shown in Fig. 3, x-ray scattered radiation images also can be determined given temporally ~~displaced~~ shifted operation of the two x-ray systems 1 and 2, since the scattered radiation has influence in this operation as well on the

image quality of the x-ray images determined by the two x-ray systems 1 and 2. As a rule, x-ray scattered radiation images for the correction of the x-ray images determined by the two x-ray systems 1 and 2 therefore are also acquired dependent upon the type of operation of the x-ray device, i.e. with regard to the temporal displacement of the acquisition of x-ray images.